

Why Cherenkov Emission During Radiotherapy is Not Strongly Dependent on Beam Energy

S. DECKER¹, D. ALEXANDER¹, R. HACHADORIAN¹, R. ZHANG^{1,3,4}, D. GLADSTONE^{1,3,4}, P. BRUZA^{1,2}, B. POGUE^{1,2,4}

¹Thayer School of Engineering, Dartmouth College, Hanover, NH USA, ²DoseOptics LLC, Lebanon, NH USA, ³Geisel School of Medicine, Hanover, NH USA, ⁴Norris Cotton Cancer Center, Dartmouth-Hitchcock Medical Center, Lebanon, NH USA

INTRODUCTION

Cherenkov radiation is the emission of light in a dielectric medium when a charged particle travels faster than the phase velocity of light in that medium. During radiotherapy, Cherenkov light is generated within a patient's tissue, approximately proportional to the delivered dose¹, and is emitted from the patient's surface (Fig. 1). This light can be captured with intensified cameras as a noninvasive method to visualize dose deposition in real time^{2,3} (Fig. 2).

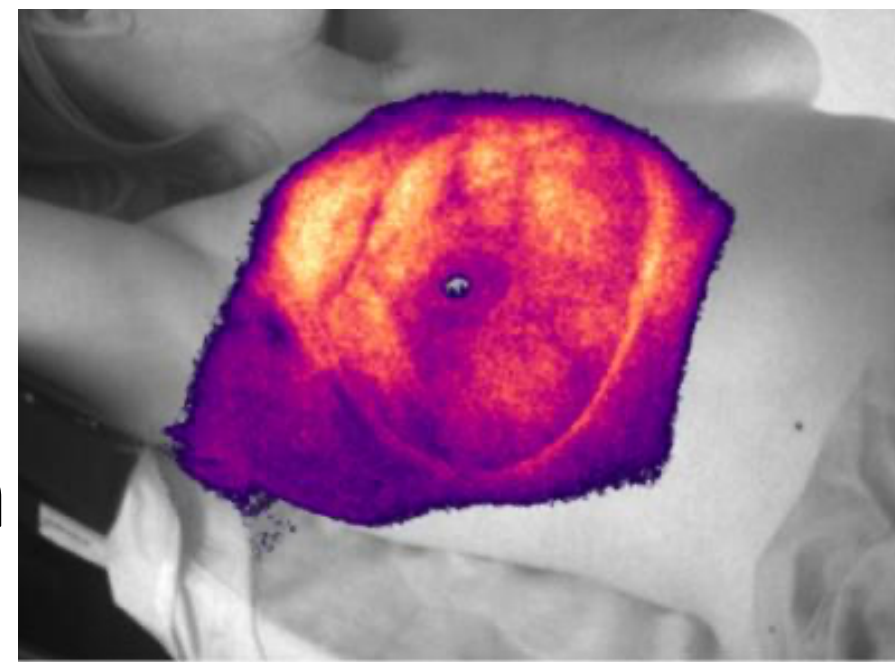


Fig. 1

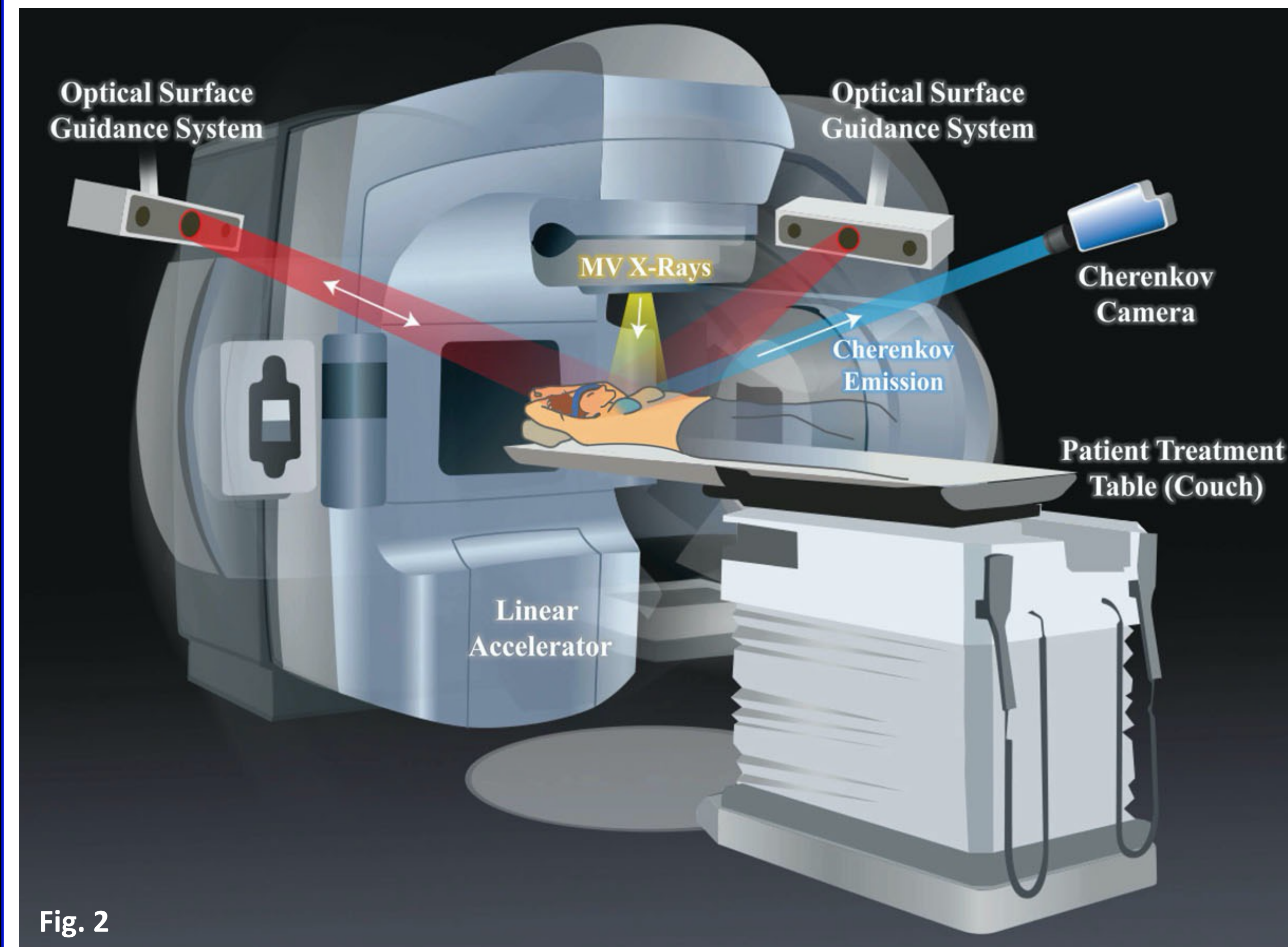


Fig. 2

Though Cherenkov light generation within tissue is strongly dependent on beam energy, it has remained a mystery why the intensity of emitted light appears to be nearly constant when treating at different energies (Fig 3.). In this study, the effects of various beam and tissue properties on the Cherenkov emission were examined in an effort to explain this observed phenomenon.

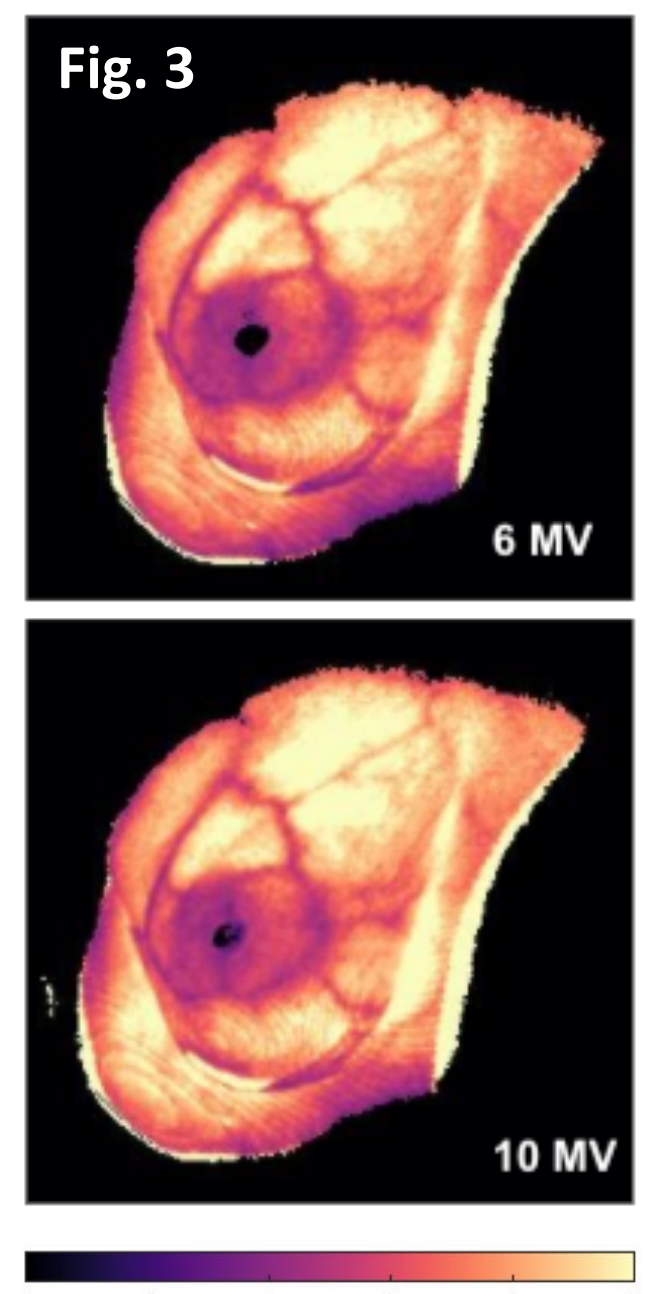


Fig. 3

AIM

To understand why the Cherenkov signal emitted during radiotherapy is not strongly dependent on treatment beam energy.

THEORY

Following diffusion theory solutions, the emitted Cherenkov signal was derived as a function of the dose build-up slope and tissue optical properties.

R: Emitted Cherenkov signal
 ϕ : Isotropic fluence rate
 k_1 : surface dose
 k_2 : build-up slope
D: diffusion coefficient
 μ_{eff} : effective attenuation coefficient

$$R_D = -D \frac{\partial \phi(r)}{\partial z} \Big|_{z=0} \quad (1)$$

$$\phi(z) = \left(\frac{1}{2D \mu_{eff}} e^{-\mu_{eff}(z)} \right) * (k_1 + k_2 z) \quad (2)$$

METHODS

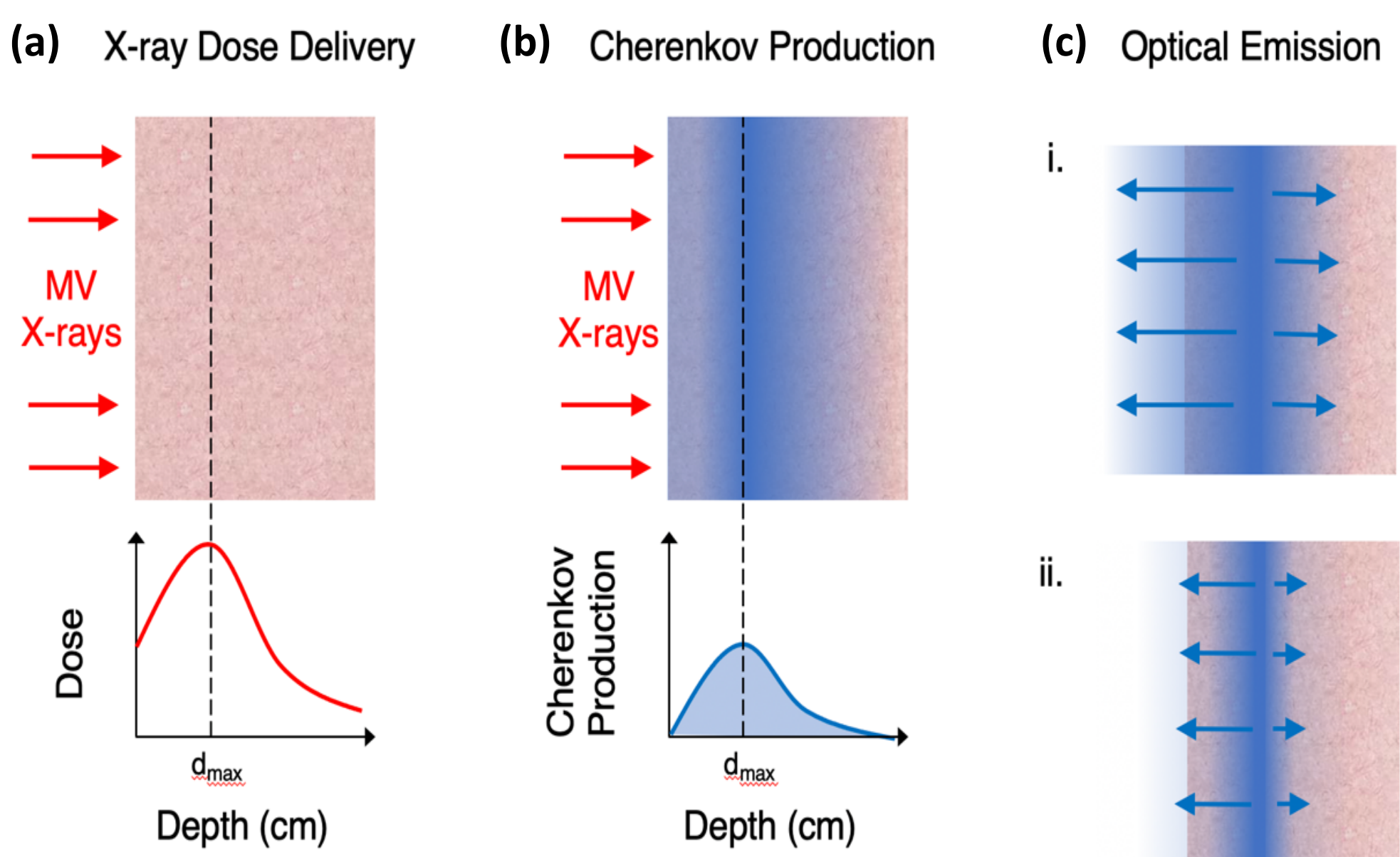


Fig. 4 A linear accelerator irradiates various tissue phantoms of different optical properties with 6, 10, and 18 MV x-rays (a) and dose is deposited as a function of depth, represented qualitatively by the graph. The depth at maximum dose, d_{max} , is also the point of maximum Cherenkov light generation (b). As tissue optical properties vary (c), so does the amount of light that escapes the surface.

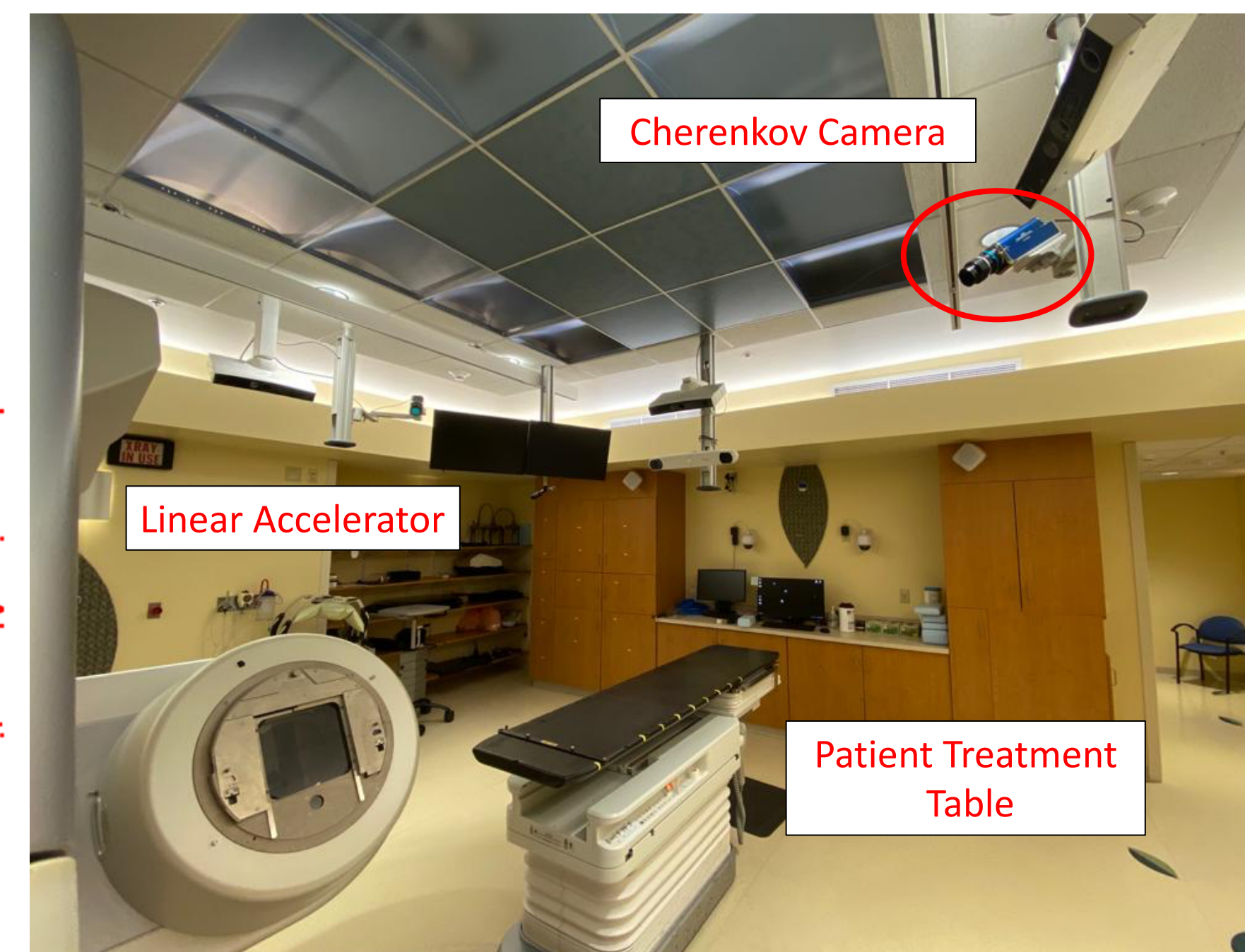


Fig. 5 The Cherenkov emission is captured with an intensified CMOS camera that is fixed in the treatment room for clinical imaging. Each phantom was irradiated top-down for entrance beam surface imaging, as well as from underneath for exit surface imaging. Phantoms were built with the thickness of the depth of d_{max} for each energy.

CONCLUSIONS

The results of this study explain why Cherenkov emission during radiotherapy is not strongly dependent on beam energy, despite greater Cherenkov photon generation at higher energies¹. Quantifying the effects of various beam properties is a progressive step towards verifying surface-dose delivery with Cherenkov light imaging during radiation therapy treatments in real-time.

RESULTS

Consistent with clinical images (Fig. 3), the Cherenkov emission from the phantom's beam entrance surface was independent of energy (a). At the beam exit surface, where there is no dose build-up region, the Cherenkov emission increased as a function of beam energy due to increased light generation¹ (b). Normalizing the entrance Cherenkov emission by approximately the number of Cherenkov photons generated revealed an inverse relationship between beam energy and the slope of the dose deposition build-up within tissue (c). **The two competing effects of increased light generation, yet slower dose build-up with increasing x-ray energy are of nearly the same magnitude, and therefore result in an approximately constant emitted Cherenkov signal from the beam entrance surface (a).**

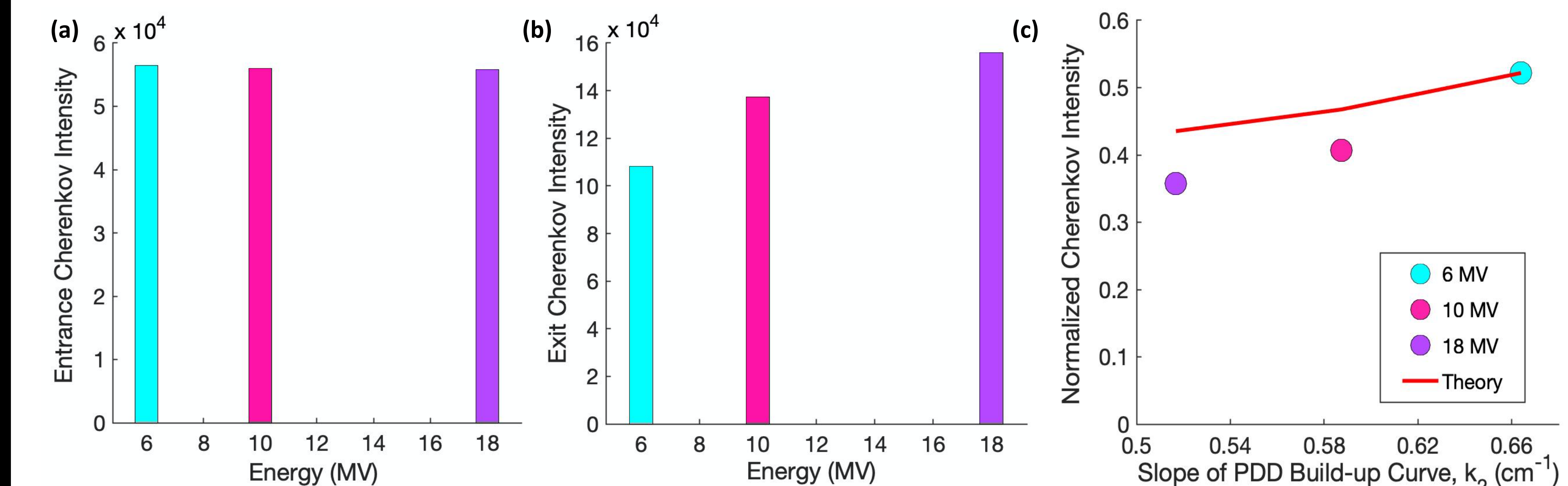


Figure 6. The intensity of Cherenkov emission from the beam entrance surface (a) and the exit surface (b) of a 1% blood / 1% Intralipid[®] diffuse liquid tissue phantom as a function of x-ray energy. Figure (c) shows the entrance Cherenkov emission intensities normalized by the exit Cherenkov intensities (proportional to the amount of Cherenkov photons produced with increasing x-ray energy) plotted as a function of the dose build-up slope. Figure (c) also shows the theoretical relative emitted Cherenkov light signal following Eqns. (1) and (2), which predict the normalized Cherenkov light that escapes the entrance surface.

ACKNOWLEDGEMENTS

The work completed in this project has been sponsored by National Institutes of Health research grant R01EB023909. The authors acknowledge the Irradiation Shared Resource at the Norris Cotton Cancer Center at Dartmouth with NCI Cancer Center Support Grant 5P30 CA023108-41.

REFERENCES

- Glaser AK, Zhang R, Gladstone DJ, Pogue BW. Optical dosimetry of radiotherapy beams using Cherenkov radiation: the relationship between light emission and dose. *Phys Med Biol*. 2014;59(14):3789-3811. doi:10.1088/0031-9155/59/14/3789
- Jarvis LA, Zhang R, Gladstone DJ, et al. Cherenkov video imaging allows for the first visualization of radiation therapy in real time. *Int J Radiat Oncol Biol Phys*. 2014;89(3):615-622. doi:10.1016/j.ijrobp.2014.01.046
- Jarvis LA, Hachadorian RL, Jermyn M, et al. Initial Clinical Experience of Cherenkov Imaging in External Beam Radiation Therapy Identifies Opportunities to Improve Treatment Delivery. *Int J Radiat Oncol Biol Phys*. 2020;0(0). doi:10.1016/j.ijrobp.2020.11.013

Decker SM, Alexander DA, Hachadorian RL, Zhang R, Gladstone DJ, Bruza P, Pogue BW. Estimation of Diffuse Cherenkov Emission from External Beam Radiation Build-Up in Tissue. (in review).

Figure List

Figures 1&2. Hachadorian RL, Bruza P, Jermyn M, Gladstone DJ, Pogue BW, Jarvis LA. Imaging radiation dose in breast radiotherapy by X-ray CT calibration of Cherenkov light. *Nat Commun*. 2020;11. doi:10.1038/s41467-020-16031-z

Figure 3: Cumulative Cherenkov images taken during whole-breast radiation therapy at DHMC NCCC. All patients provided informed consent in this IRB approved study.

Figure 5. Photo by courtesy of Daniel A. Alexander.

CONTACT INFORMATION

Savannah Decker
Graduate Student—Pogue Lab
Thayer School of Engineering
Dartmouth College
Savannah.M.Decker.TH@dartmouth.edu
Cell: 315-939-0987

Prof. Brian Pogue, PhD
MacLean Professor of Engineering
Professor of Surgery, [Geisel School of Medicine](http://www.dartmouth.edu/geisel)
Co-Director, [Translational Engineering in Cancer Research Program](http://www.dartmouth.edu/translational-engineering), Norris Cotton Cancer Center
Brian.W.Pogue@dartmouth.edu
Lab: (603) 646-3861